

Variations in speech-in-noise thresholds as it relates to central inhibitory function

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1. INTRODUCTION

- Speech understanding in the presence of background noise is a major issue for individuals with hearing impairment
- Aging, in addition to hearing loss, affects central inhibitory function¹, and could potentially contribute to poor speech in noise (SiN) performance
- Cortical alpha (7.5-12.5Hz) activity is an indirect measure of central inhibition and is believed to contribute to a person's ability to understand SiN^{4,6,7}
- The relationship between Alpha rhythms and SiN perception have been studied^{6,7}, and resting state or reference alpha power activation has been positively associated with performance in other cognitive tasks^{2,5,8}
- Less is known about how individual resting state alpha relates to SiN performance
- Increased alpha activity is believed to aid in the suppression of background noise, thus allowing the listener to focus on the relevant signal (speech)⁷
- Purpose of the present study was to examine if an individual's inhibitory function, as defined by their resting state alpha activity, would contribute to signal-to-noise ratio (SNR) thresholds

2. METHODS

- Participants: Adult bilateral hearing aid users (n = 15), age 59-81 (mean = 68.3)
- Mild-moderate hearing loss
- All subjects wore hearing aids for at least two years prior to testing
- All testing was performed unaided
- Baseline resting state activity was recorded in a silent, dark environment

EEG Recording

- 64 channel Neuroscan system
- Online sampling rate of 1000Hz
- Alternating 2 minute blocks with eyes open/eyes closed
- Three blocks per condition

SiN Testing

- Speech: presented in sound field, single speaker 0° azimuth, 1m away
- Noise: 4-talker babble in foreign languages (ISTS)³
- English sentences presented at -10 to +15 SNR in 5dB steps
- SNR-50 thresholds were estimated by fitting a psychometric function to correct or incorrect responses on the Hearing in Noise Test (HINT)
- SNR-50 is the dB threshold where an individual answers 50% of the words correctly
- Noise held constant at 65dB SPL while sentences varied adaptively in 5dB steps

Data Analysis Pipeline

- Alpha power was calculated using Fieldtrip, a MATLAB based toolbox
- Trials were defined as eyes open or eyes closed
- Bandpass filtered 0.5-50Hz
- Down sampled to 250Hz
- Independent Component Analysis (ICA) was used to remove biological artifacts such as eye blinks, eye movements, and electrocardiogram (EKG; Fig.1), as well as noisy channels (i.e. 60Hz)
 - ICA was conducted over the continuous EEG recording
 - Average of 3-5 components removed per subject

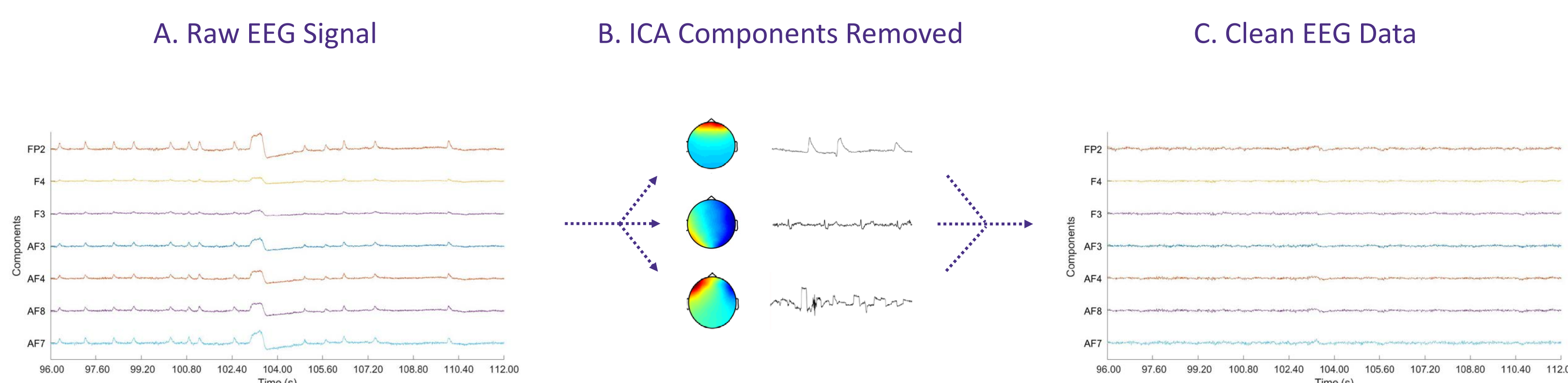
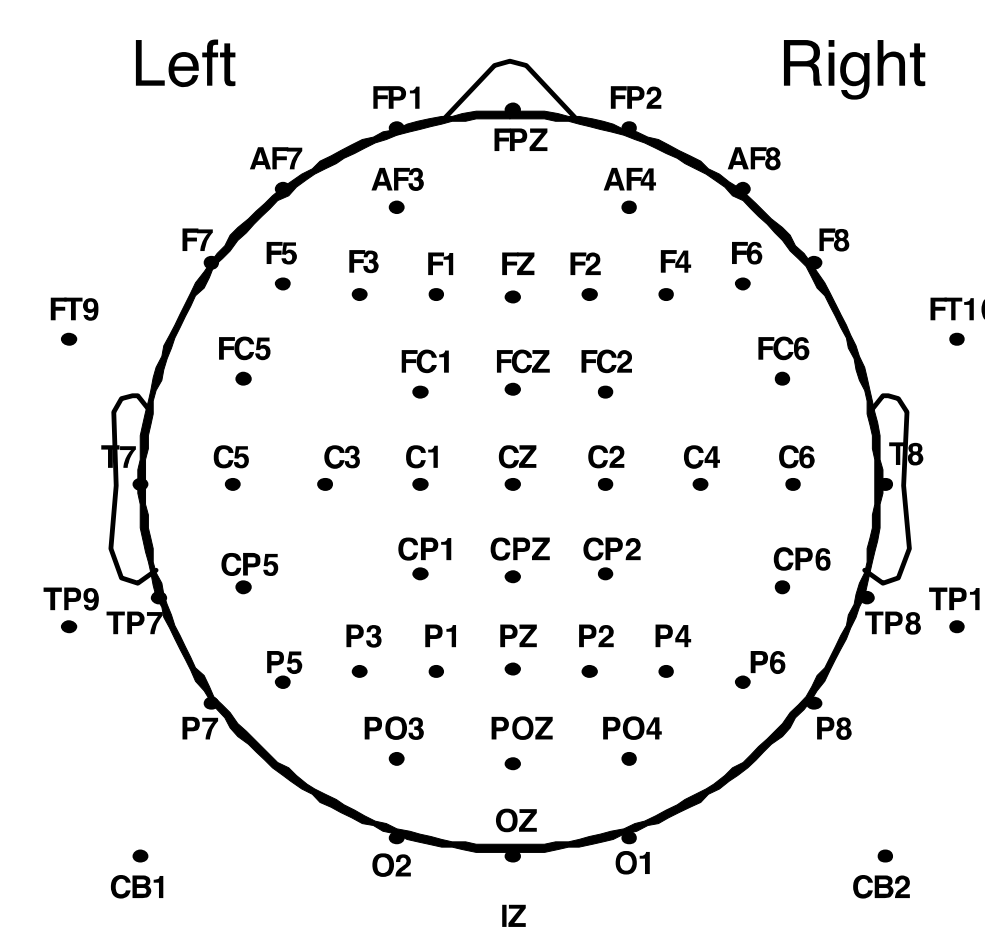


Figure 1. ICA artifact removal pipeline. A) Select channels showing raw EEG data bandpass filtered 0.5-50Hz. Note the eye blink artifacts across channels, and a large eye movement at ~103 seconds. B) Topo-maps of three independent components (ICs) and their distinct waveforms: eye blinks, EKG, and eye movements respectively. C) EEG data after removal of the ICs. Note the contrast to the raw waveform.

3. RESULTS

Resting state alpha activity varied among subjects

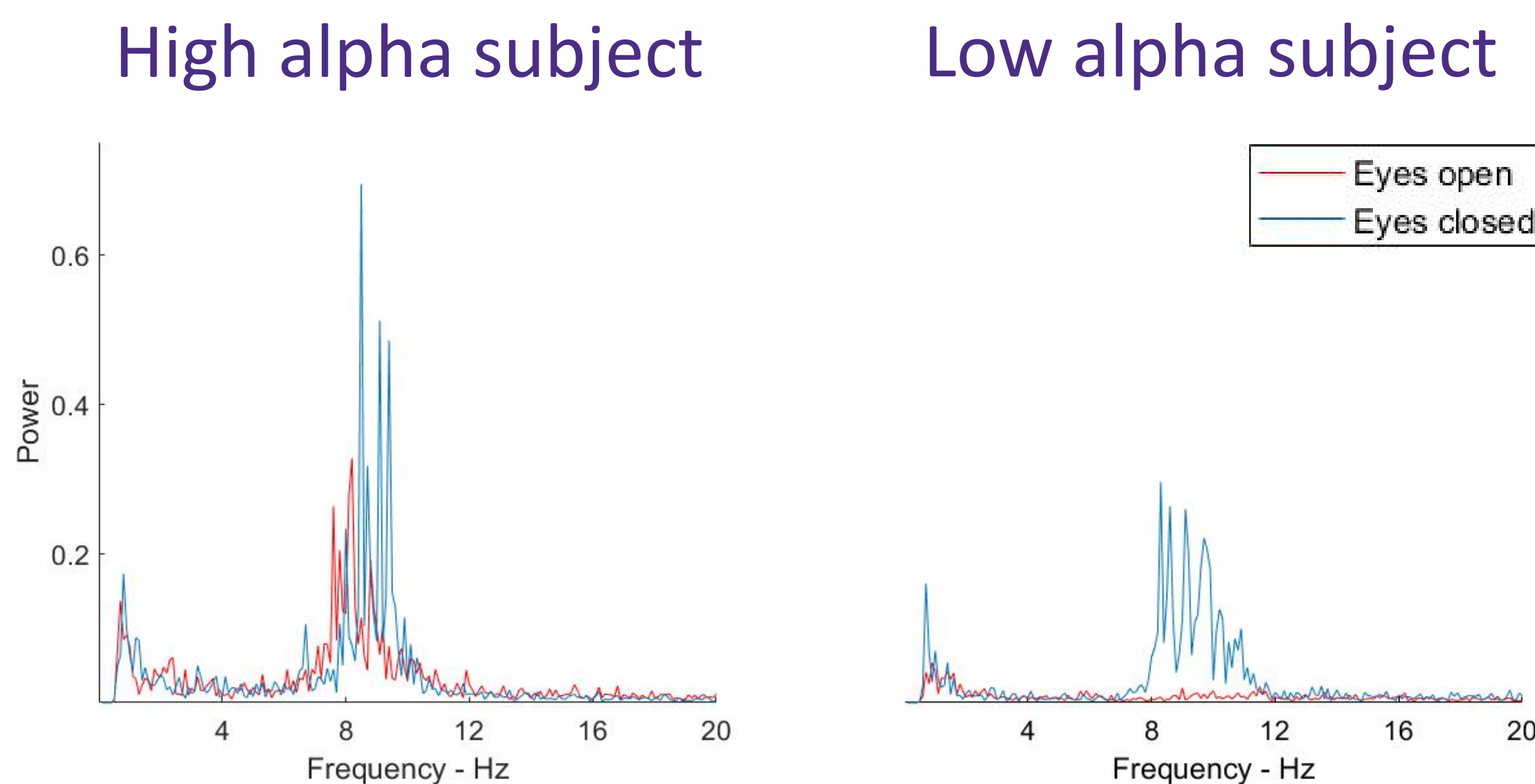


Figure 2. Fast Fourier Transform (FFT) for two subjects across occipital channels: OZ,O1,O2,POZ,PO3,PO4 in both the eyes open and eyes closed condition.

Time frequency data averaged across occipital channels: OZ,O1,O2,POZ,PO3,PO4

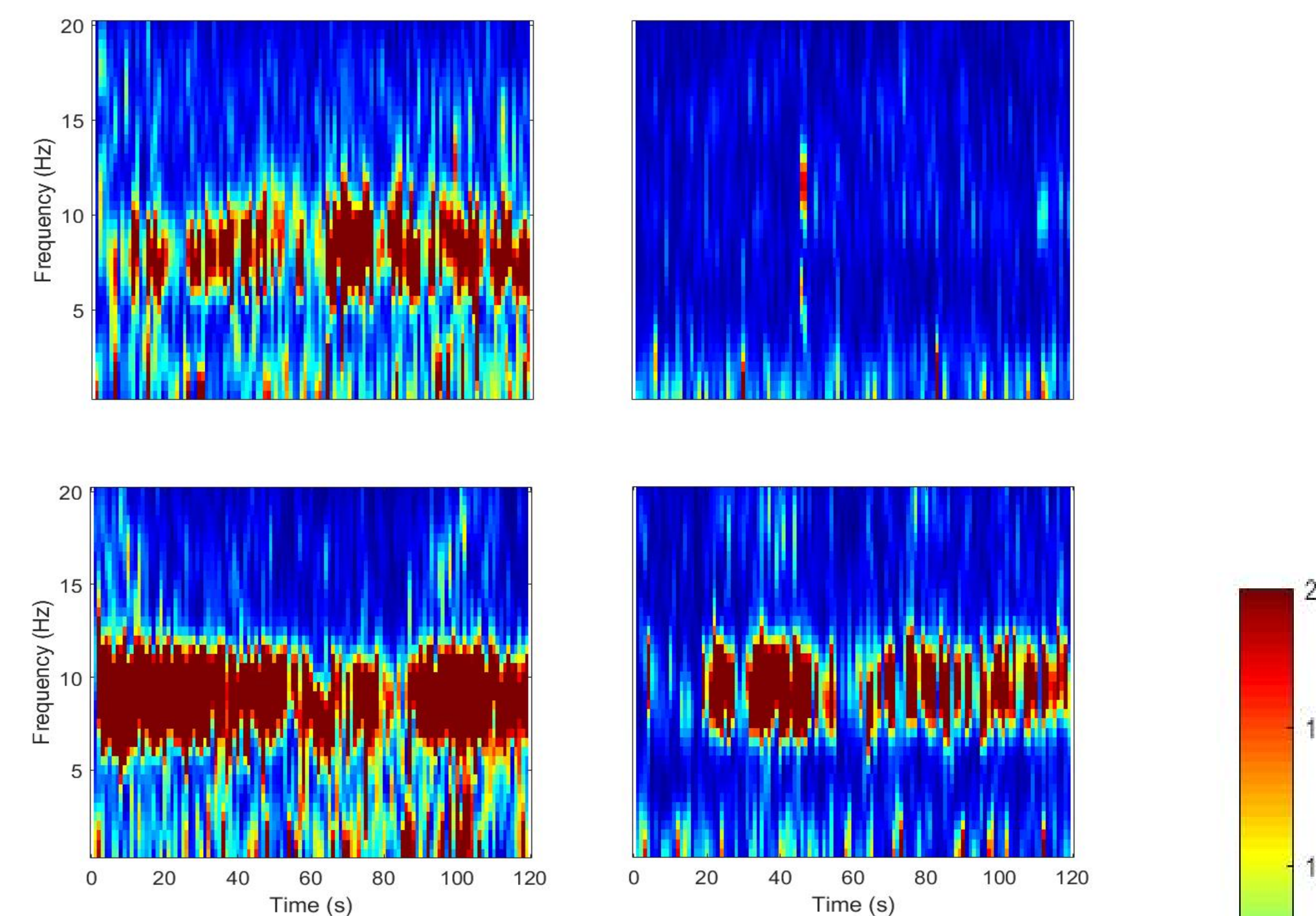


Figure 3. Time frequency data for two subjects. The top row of panels shows oscillatory activation in the eyes open condition, and the bottom row eyes closed, for each subject respectively. Oscillatory activity is shown with the greatest activation in the alpha band (7.5-12.5Hz).

Topographical representation of alpha band power

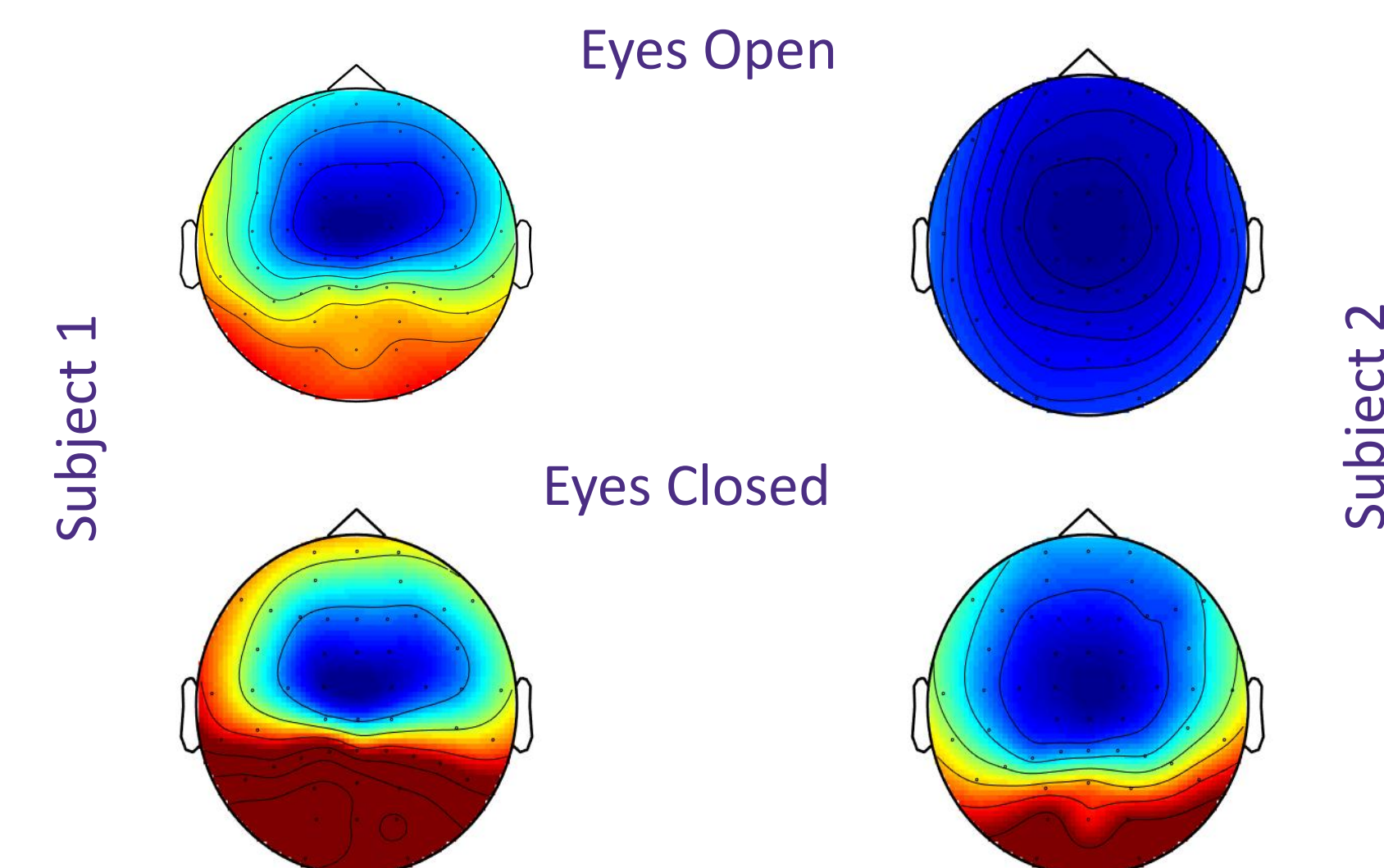


Figure 4. Oscillatory alpha band activity estimated at the level of the scalp. Top row of panels represents two subjects during the eyes open condition, and with eyes closed in the bottom row. Notice the subject differences in the eyes open condition, and the similarities during eyes closed. Greater differences in the eyes open condition would suggest subject 1 has higher resting state alpha power compared to subject 2, which may lead to performance differences in SNR testing (data not shown).

3. RESULTS CONTINUED

SNR thresholds significantly associate with alpha power

| | Est. co-efficient | Standard error | P-value |
|-------------------------|-------------------|----------------|---------|
| Alpha power eyes open | -30.6 | 8.4 | 0.003* |
| Alpha power eyes closed | 11.8 | 4.2 | 0.02* |

Table 1. Linear regression model ($y = \beta_0 + \beta_1 X_1 + \beta_2 X_2$) where $y = \text{SNR-50 threshold}$, $X_1 = \text{alpha power eyes open}$, $X_2 = \text{alpha power eyes closed}$, and β_0 the y intercept. Significance is indicated by *

Decreased SNR thresholds were associated with increased alpha power

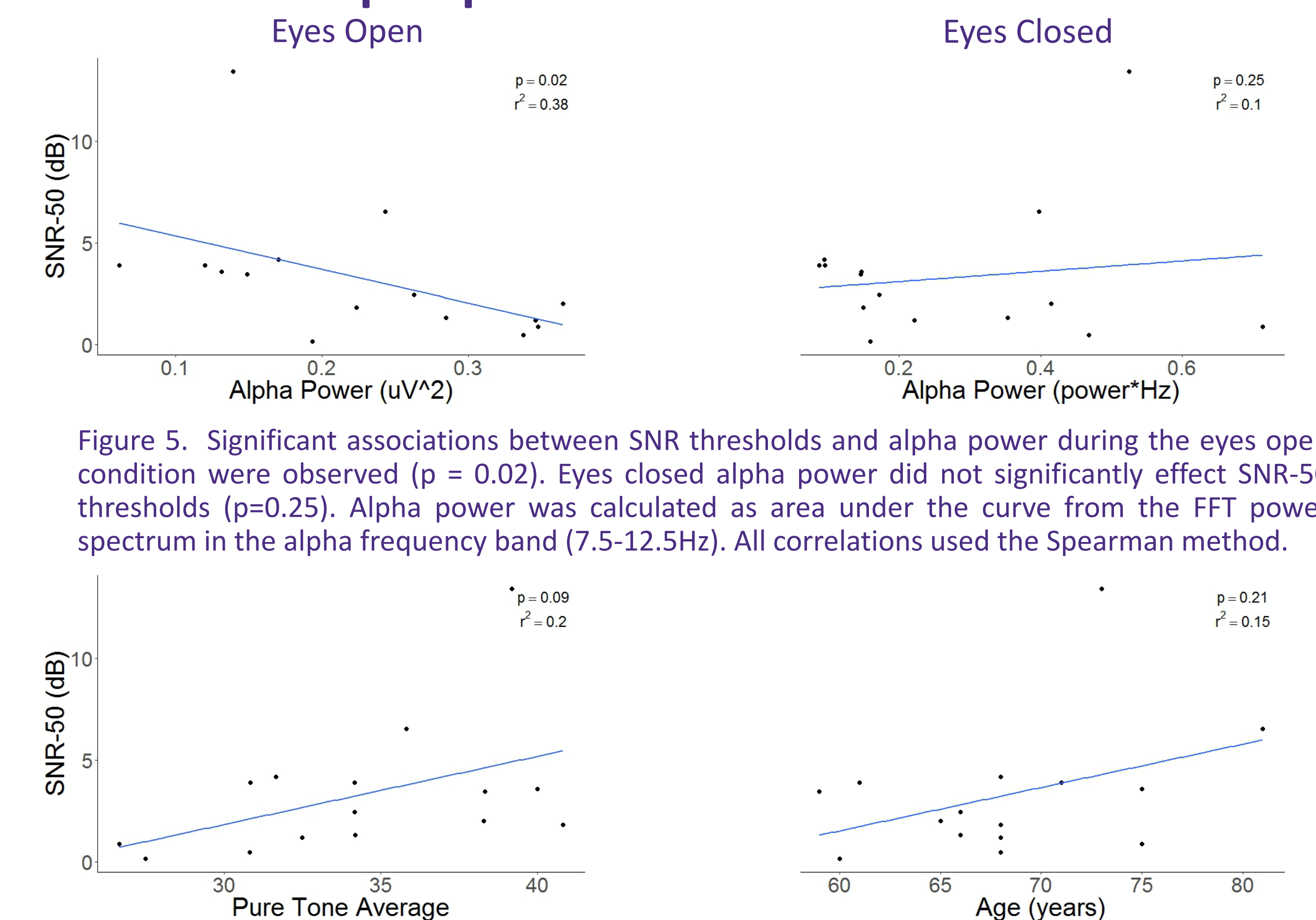


Figure 5. Significant associations between SNR thresholds and alpha power during the eyes open condition were observed ($p = 0.02$). Eyes closed alpha power did not significantly effect SNR-50 thresholds ($p = 0.25$). Alpha power was calculated as area under the curve from the FFT power spectrum in the alpha frequency band (7.5-12.5Hz). All correlations used the Spearman method.

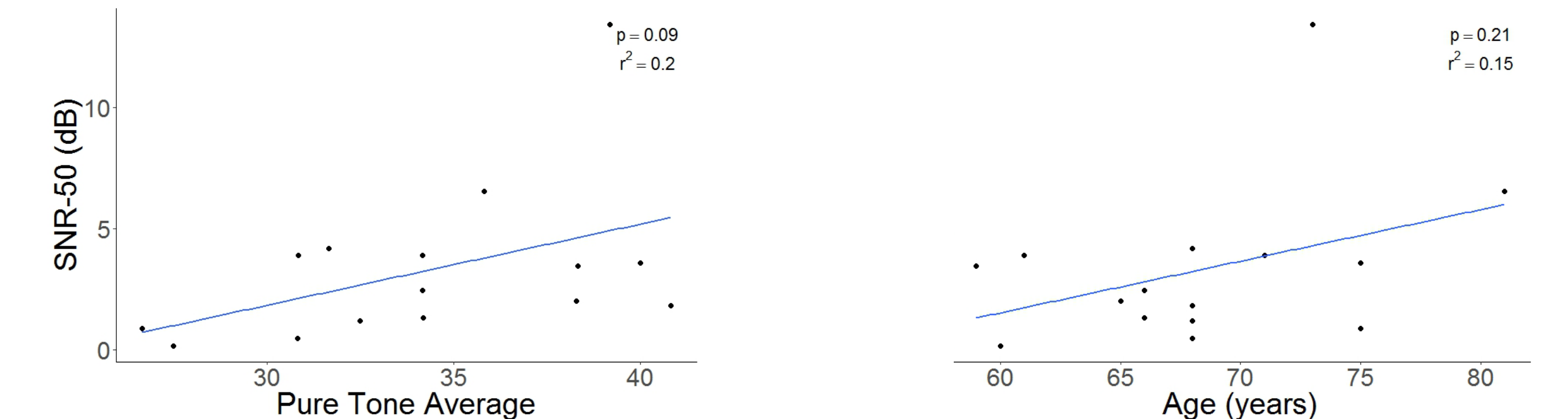


Figure 6. SNR-50 thresholds as a function of pure tone average (PTA) and age, respectively. Neither PTA or age was significant ($p = 0.09, p = 0.21$) in how they affected SNR-50 thresholds. All correlations used the Spearman method.

4. CONCLUSIONS

- Individual subject alpha power differences were observed in both conditions
- Alpha power was primarily concentrated to occipital areas
- Alpha power was greater in the eyes closed condition compared to eyes open
- SNR-50 thresholds decreased as a function of alpha power during the eyes open condition, and increased during eyes closed
- Audibility and age did not significantly contribute to SNR-50 thresholds
- EEG alpha power may be predictive of SNR-50 threshold outcome measures

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